

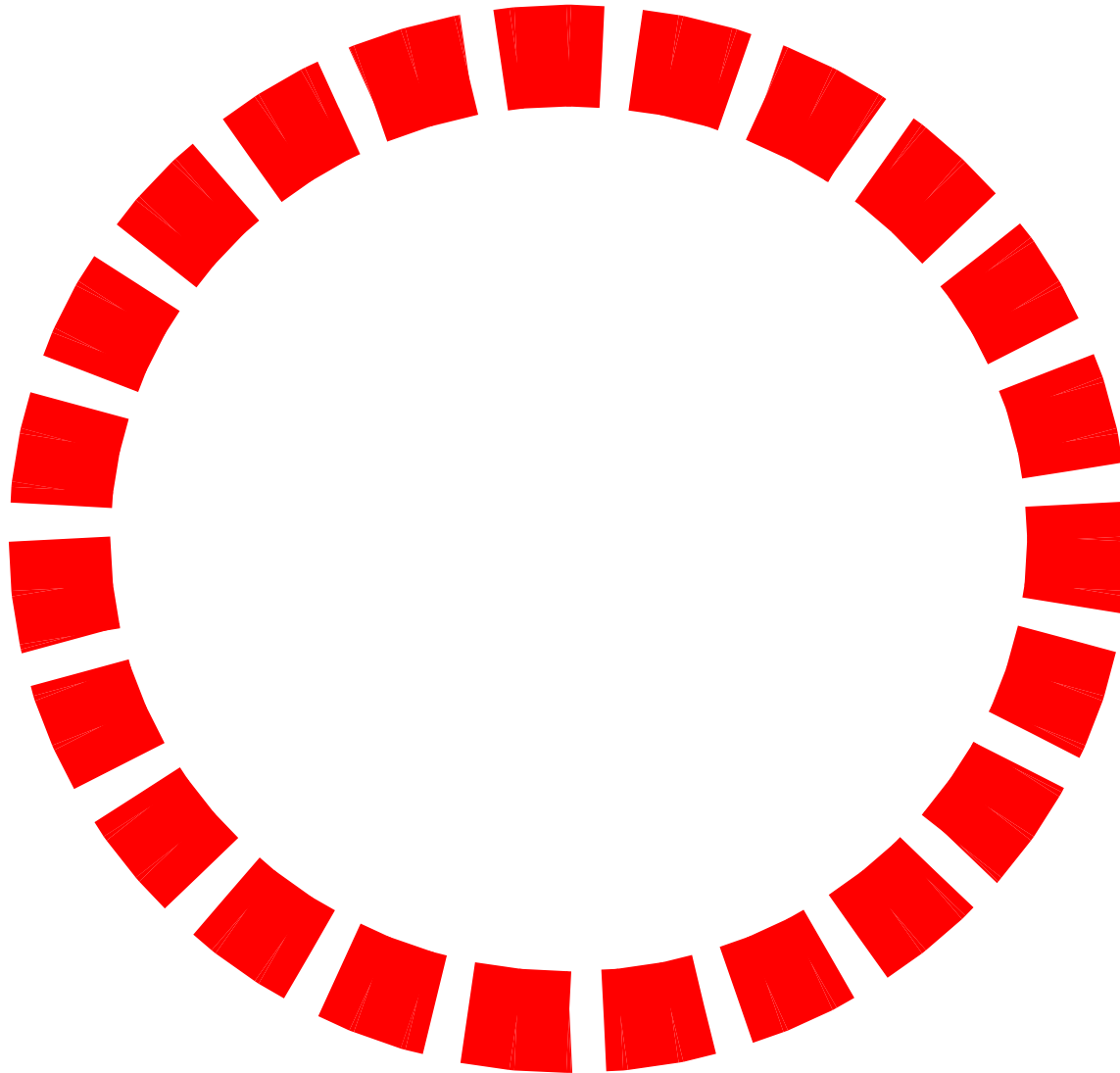


# A Silicon detector probe for high-resolution PET imaging

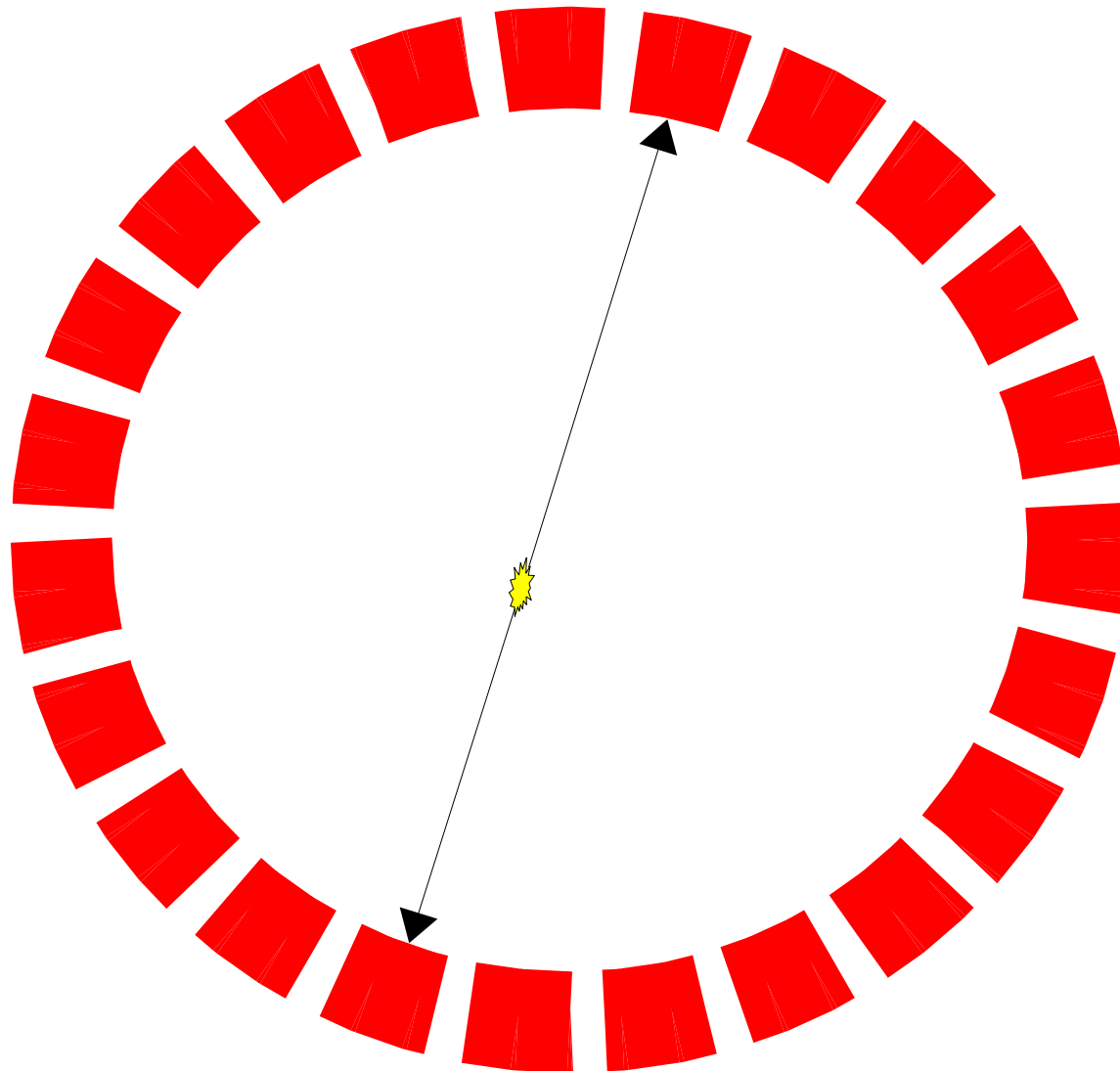
K. Brzeziński

Instituto de Física Corpuscular, CSIC/Universitat de València,  
Valencia, Spain.

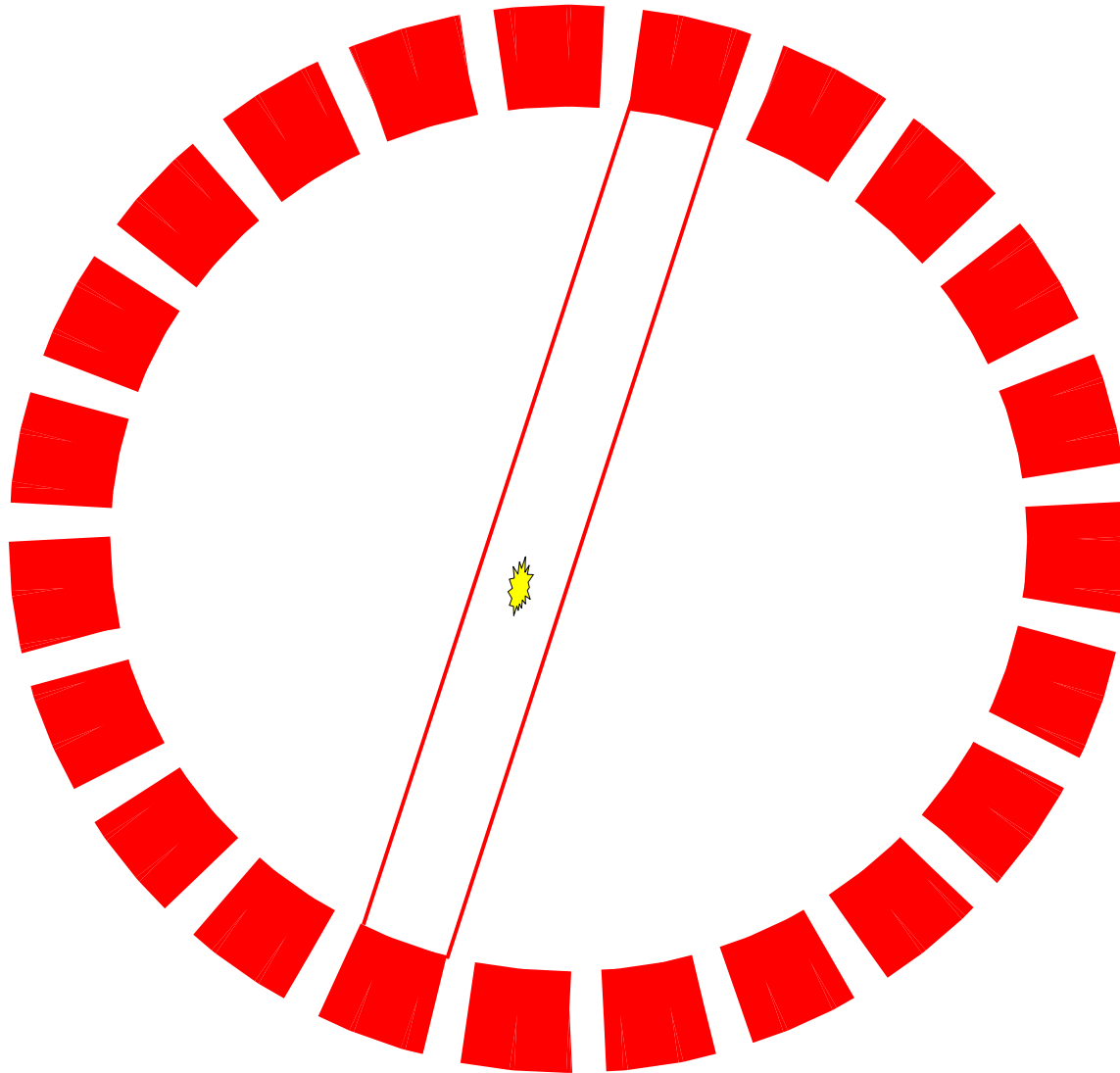
# PET insert concept



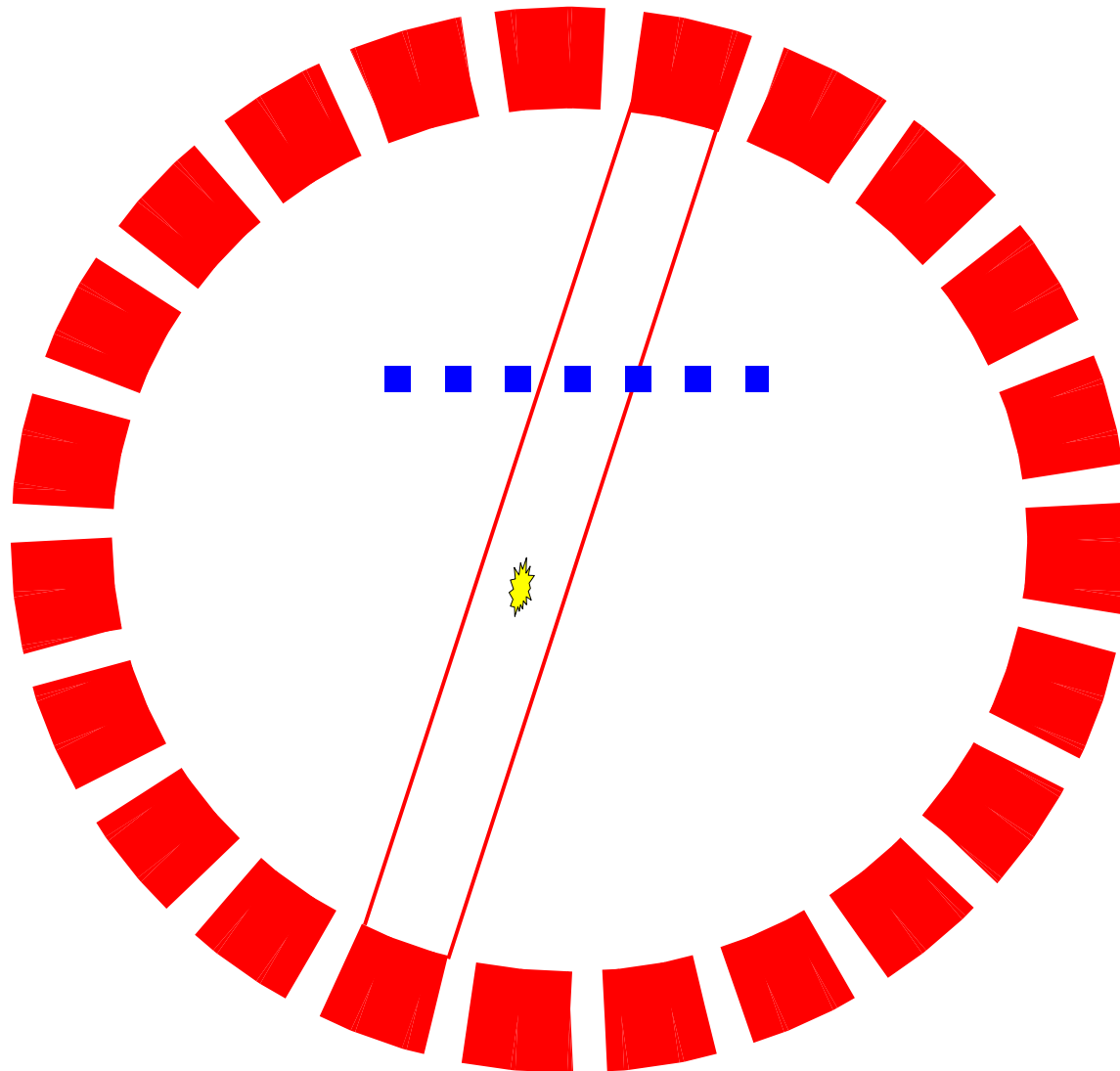
# PET insert concept



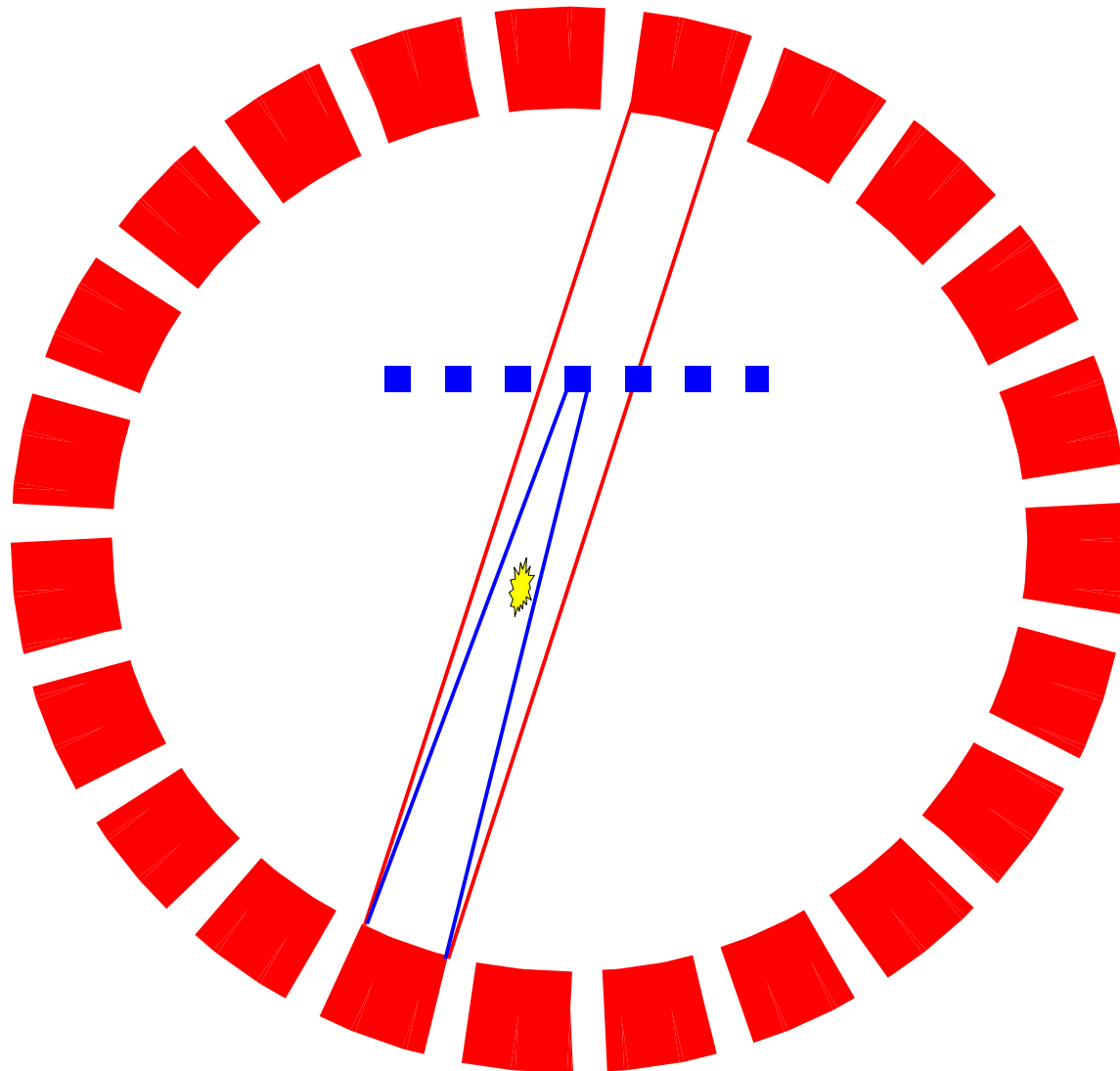
# PET insert concept



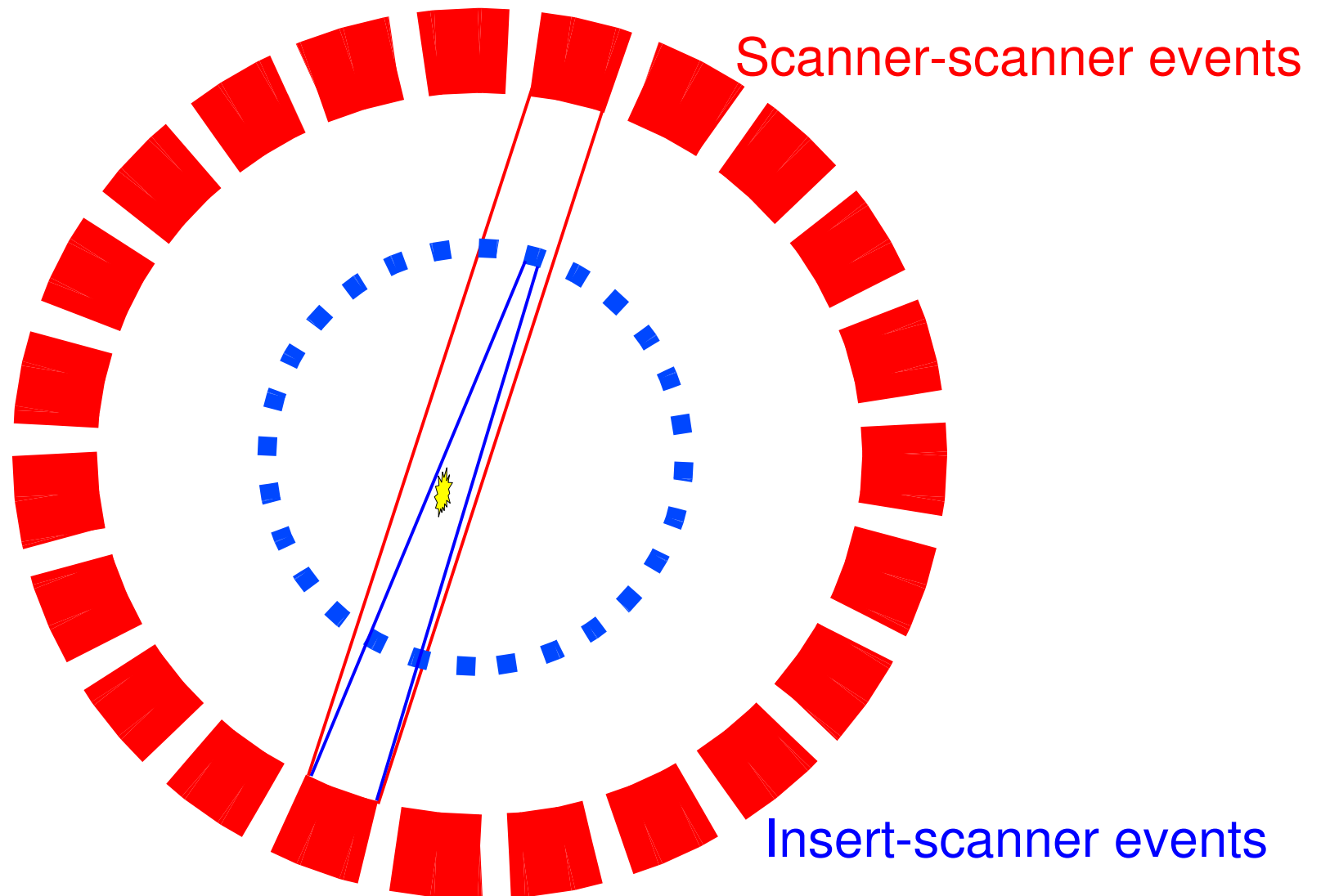
# PET insert concept



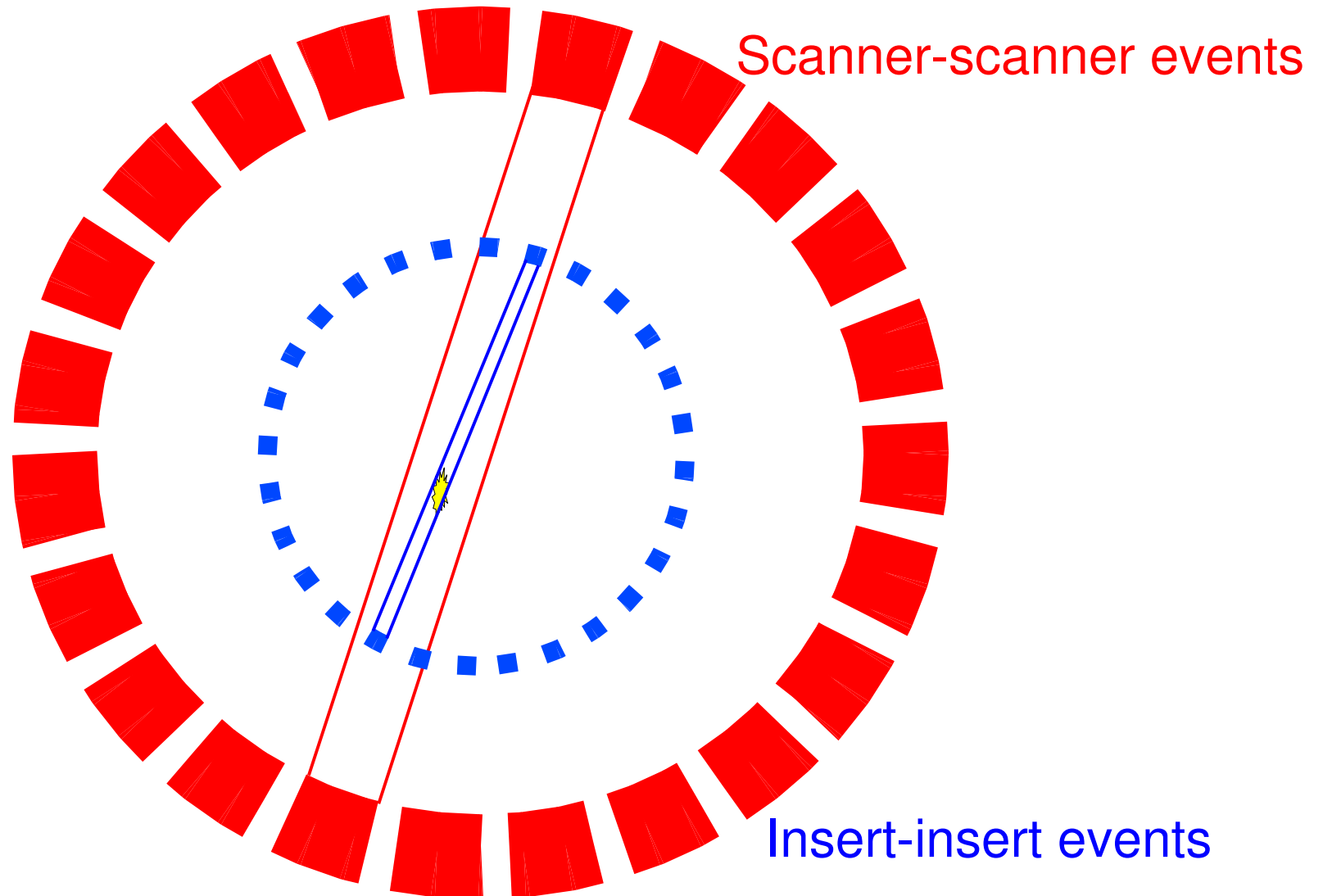
# PET insert concept



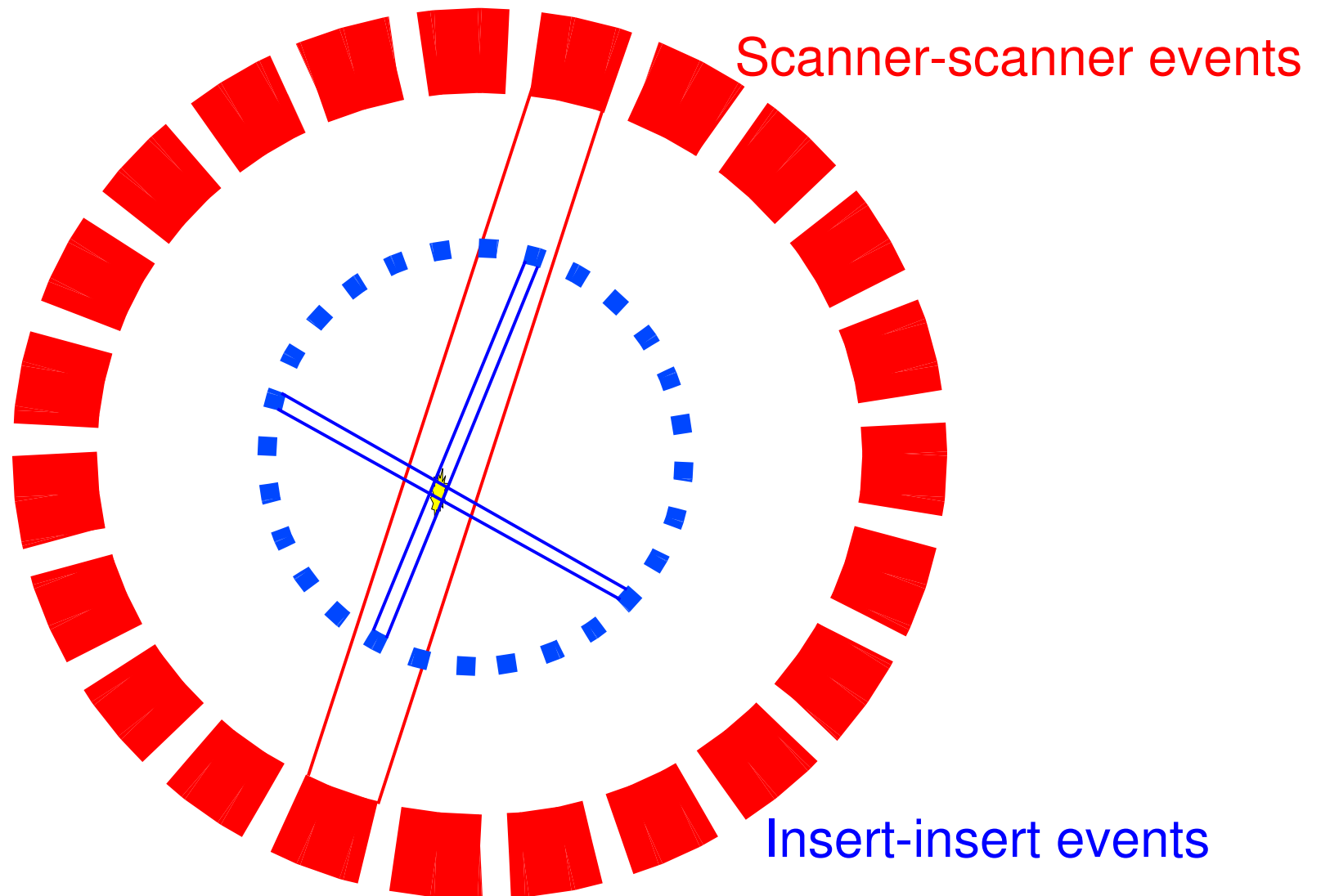
# High-resolution inserts: ring geometries



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# High-resolution inserts: ring geometries

**Improved spatial resolution** observed through a decrease in FWHM.

## Simulation studies:

Clinical scanner + LSO insert<sup>1</sup>:

~ 64 % insert-insert events

Small animal scanner + Si insert<sup>2</sup>:

~ 85 % insert-insert events

~ 45 % insert-scanner events

## Experimental prototypes:

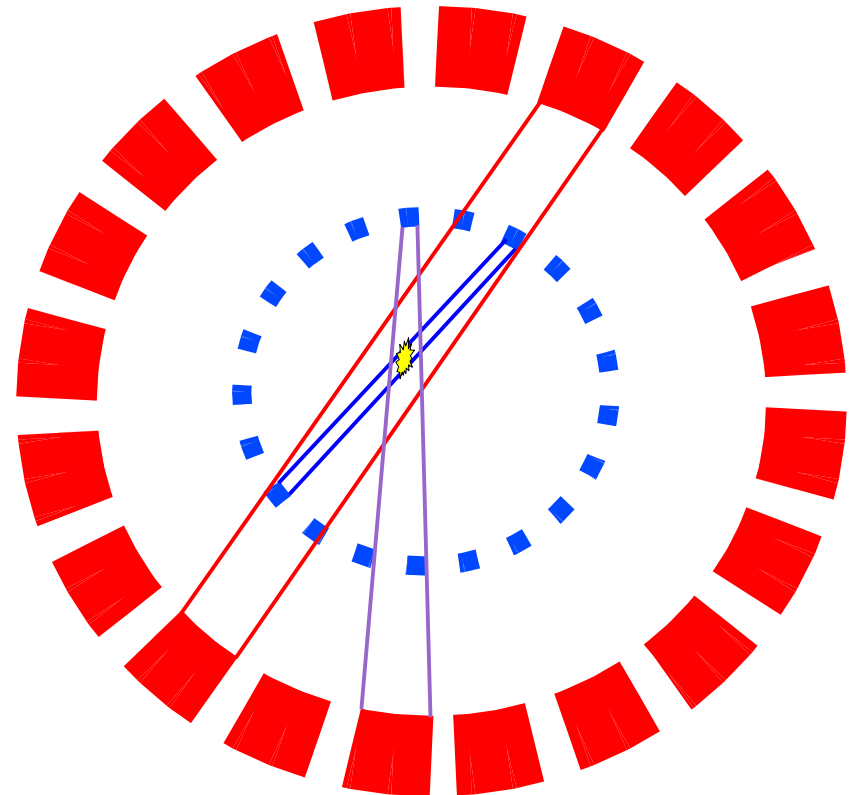
Small animal scanner + LSO insert<sup>3</sup>:

~ 33 - 41 % insert-insert events

~ 17 - 23 % insert-scanner events

Clinical PET-CT + LSO insert<sup>4</sup>:

~ 40 - 50 % insert-insert events



1. Janecek M. et al (2006)

2. Park S.J et al (2007)

3. Wu H. et al (2008)

4. Wu H. et al (2008)

# High-resolution inserts: “probe” geometries

## Advantages:

- More straight forward to adapt to an existing PET scanner.
- Focus on target region close to the face of the detector.
- Flexibility (adaptive imaging possible).
- More cost effective.

## Improved spatial resolution

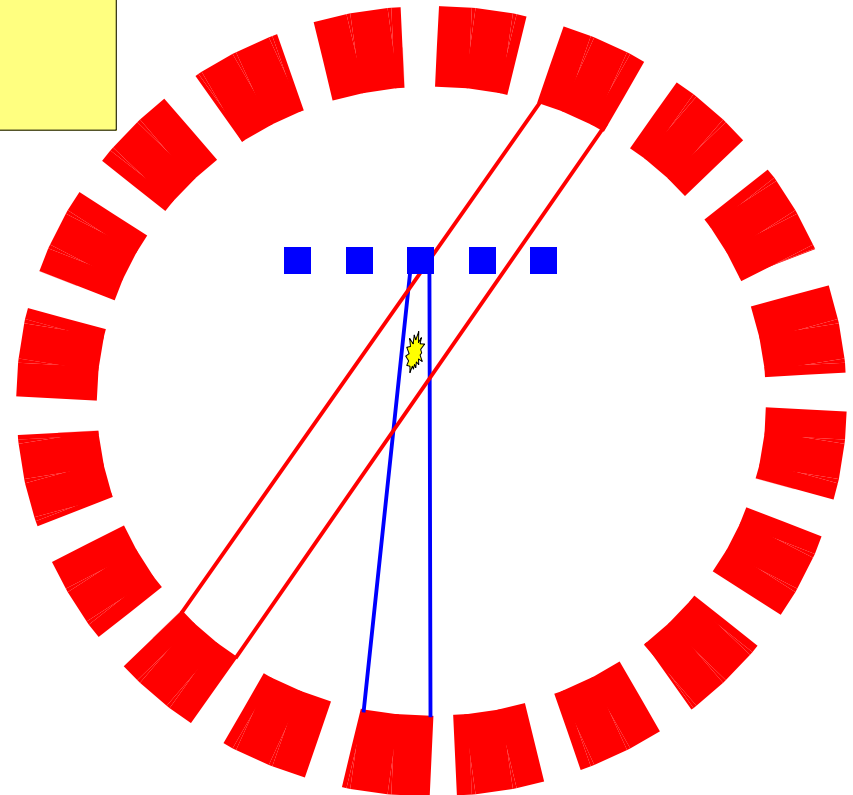
### Simulation studies:

Small animal scanner + LSO (DOI) probe<sup>1</sup>:

~ 60 % probe-scanner events

MADEIRA system:

~ 50 % insert-scanner events



1. Zhou J. et al (2009)

# The MADEIRA geometry

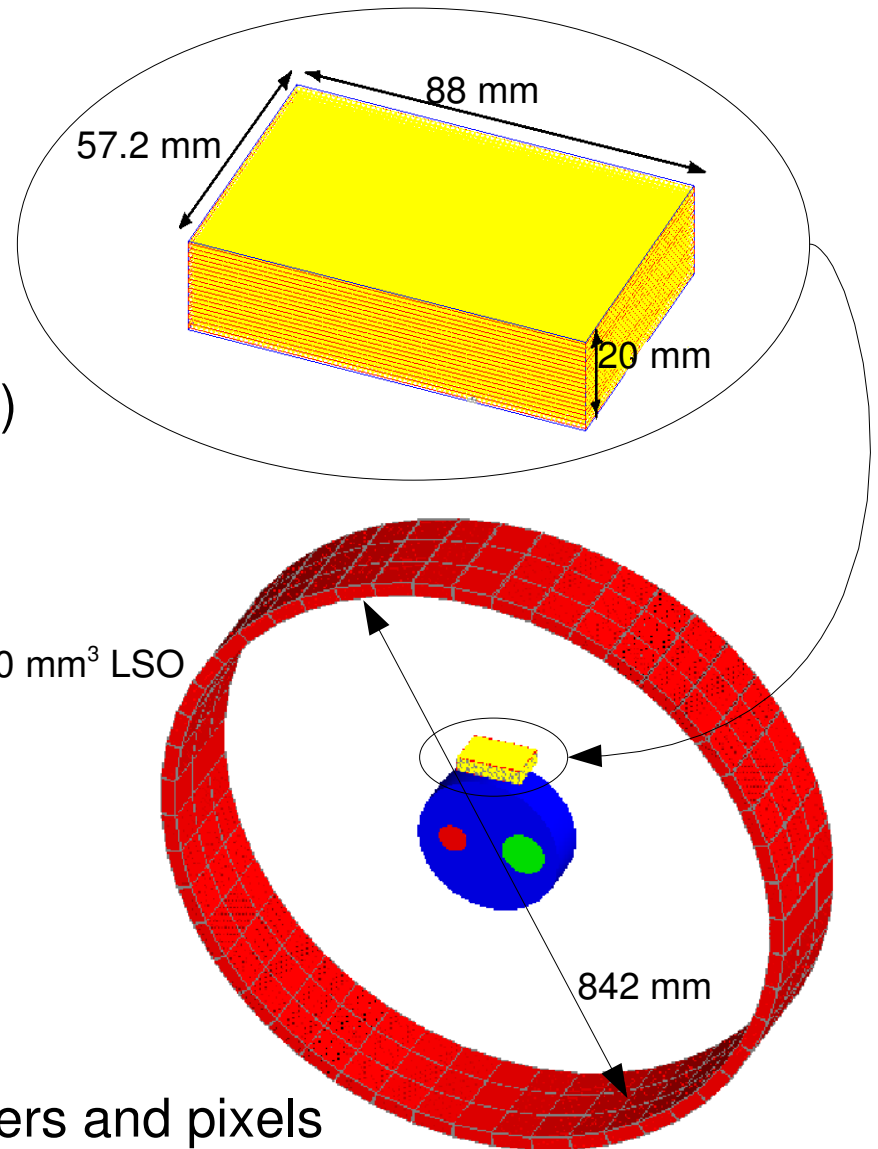
## The MADEIRA probe:

Finely pixelated silicon detectors

- Good spatial resolution
- Good energy resolution (event classification)
- Robust and compact
- Functions in magnetic fields
- Mature technology

## Monte Carlo simulations (GATE):

- 10 layers of Si (1 mm thick, 1mm spacing)
- $1 \times 1 \text{ mm}^2$  pixels in  $80 \times 52$  arrays
- Scanner modeled on Siemens Biograph64
- Experimental probe prototype has fewer layers and pixels

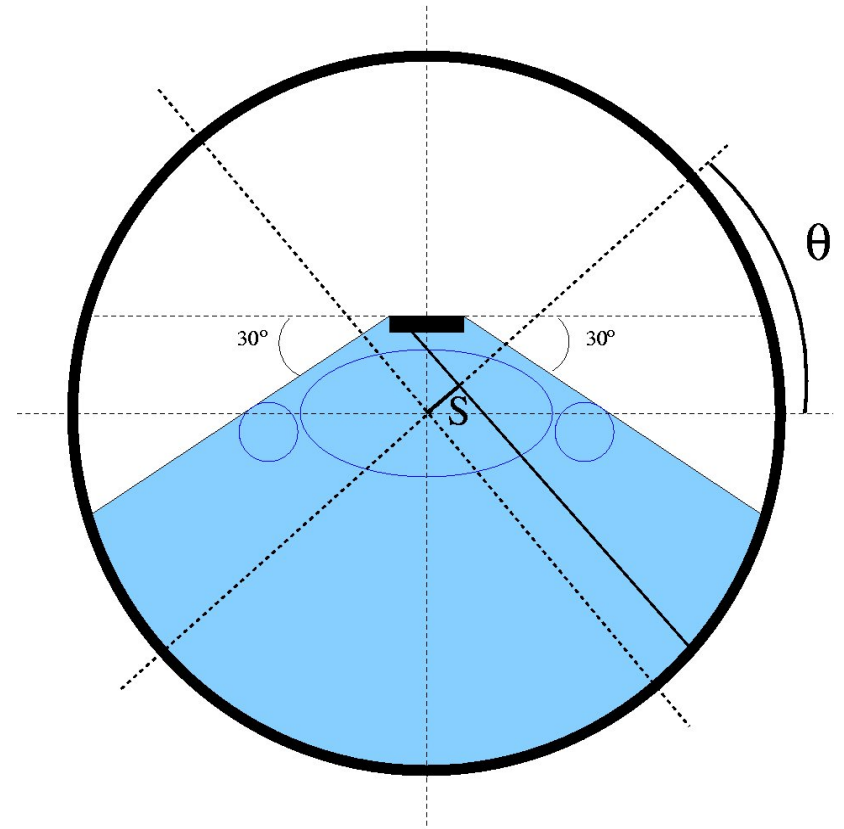


# Possible clinical application

- High resolution in localized ROI – Breast cancer imaging
- PET in mammography – An accurate tool
  - Primary tumor detection
  - Axillary staging
  - Defining extent of cancer
  - Therapy response monitoring
- High resolution may be beneficial for a number of these tasks

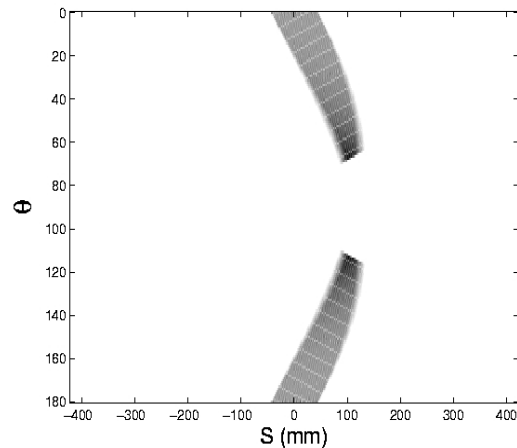
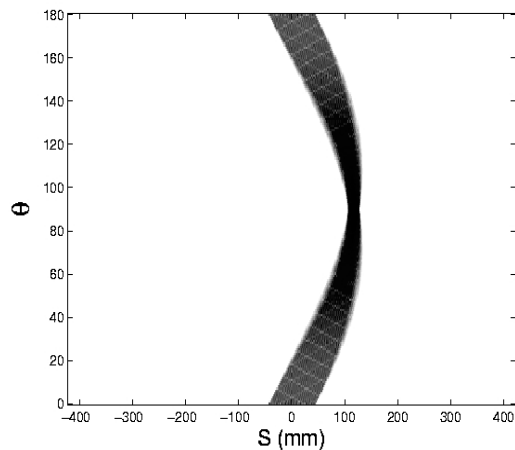
# Nature of the probe-ring data

- High resolution
- Limited angular coverage
- To be used to enhance ring-ring data
- Limited FOV
  - Other data can be “cut out”



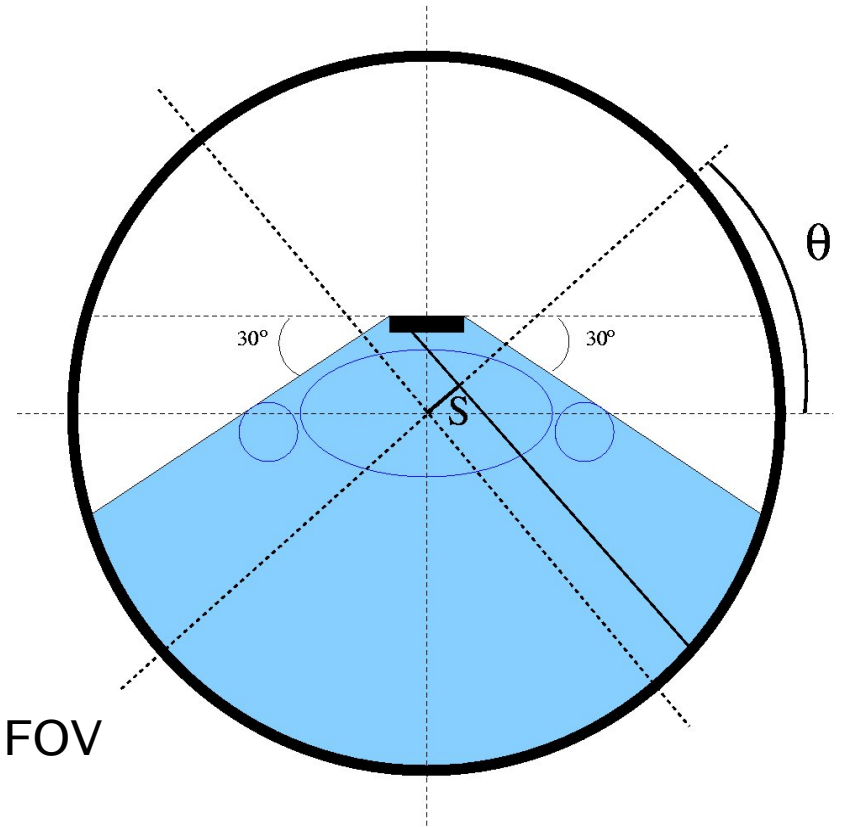
# Nature of the probe-ring data

In Radon space:



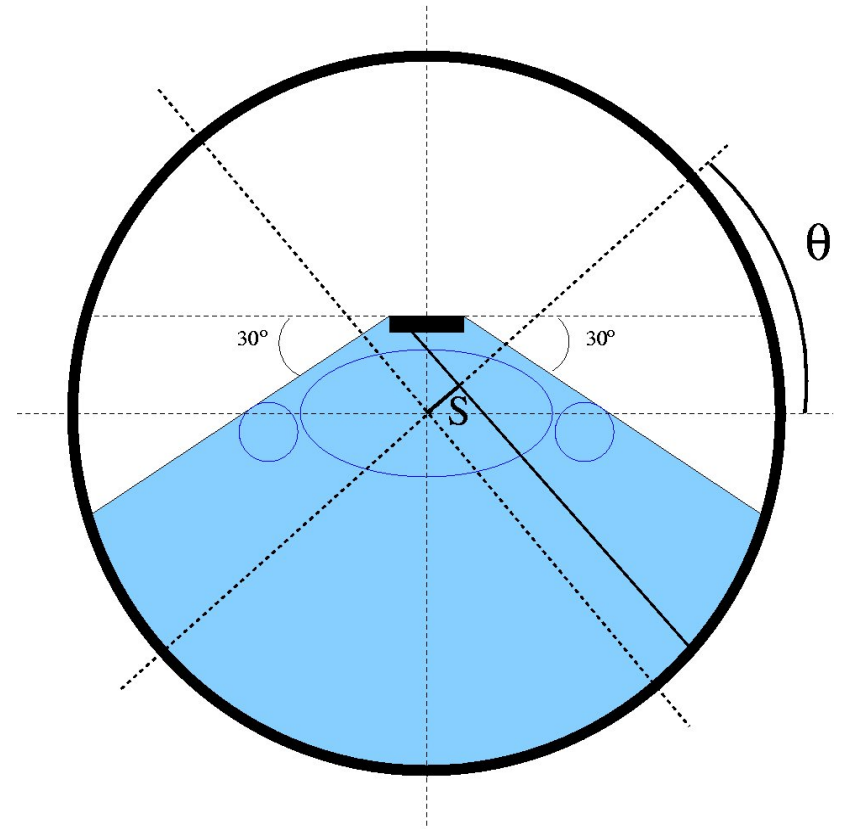
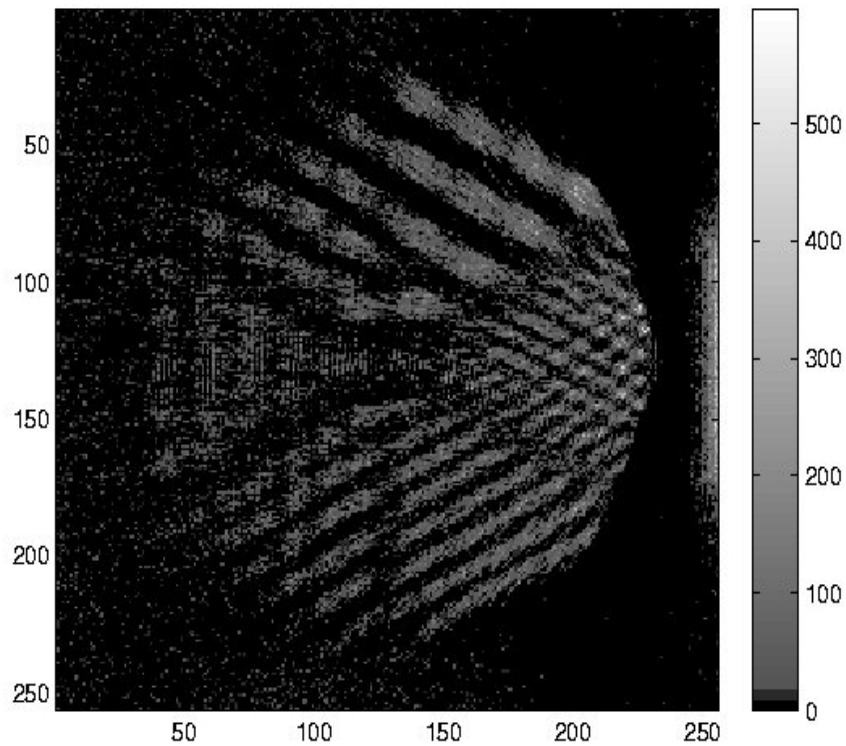
Full probe-ring FOV

Limited probe-ring FOV



# Nature of the probe-ring data

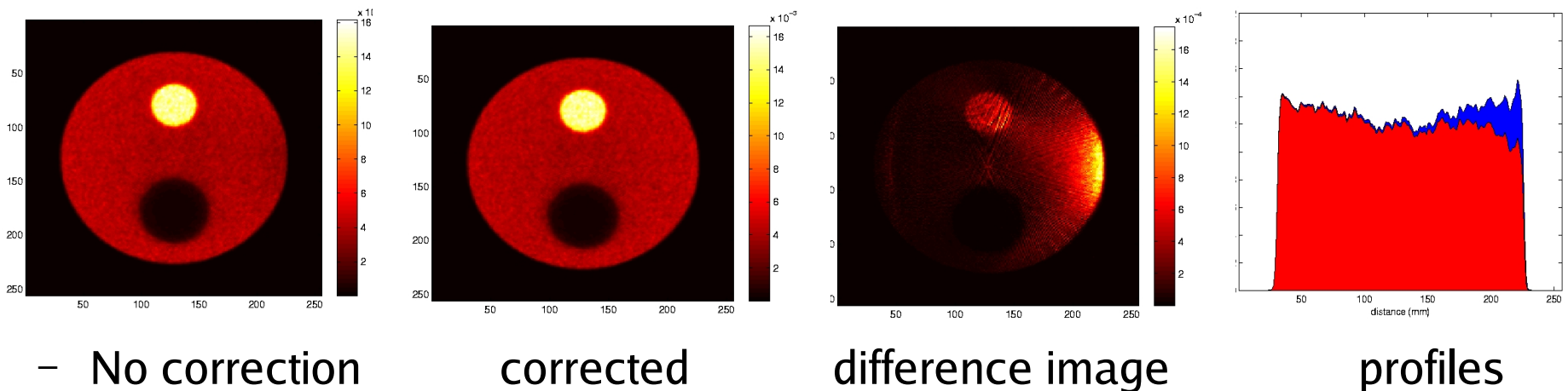
In image space:



# System modeling and image reconstruction

- ML-EM

- Abundance of possible measurements-> list-mode

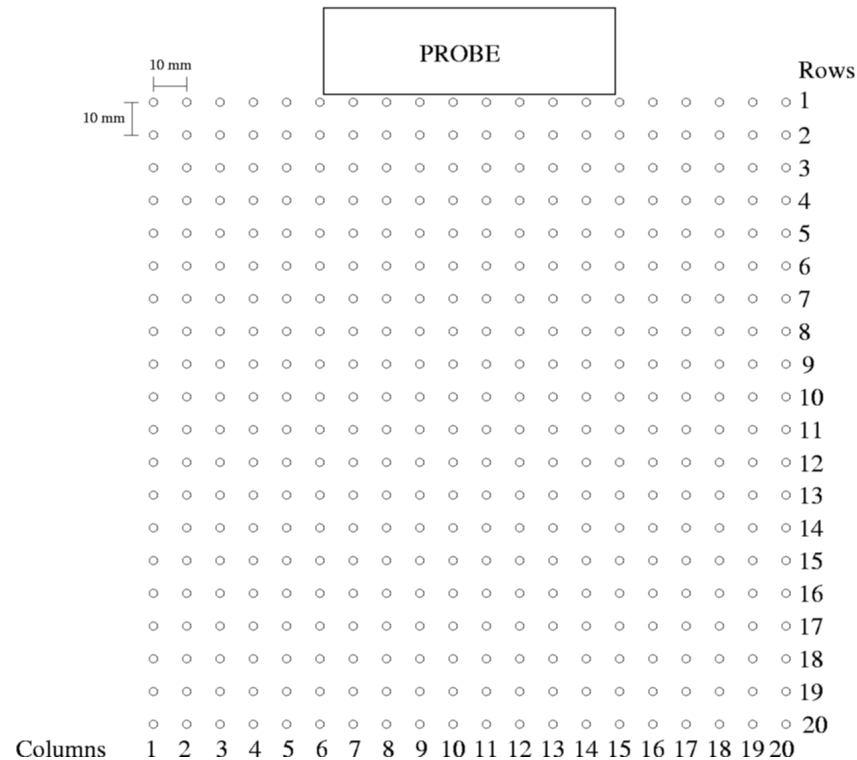


- Probe attenuation effects

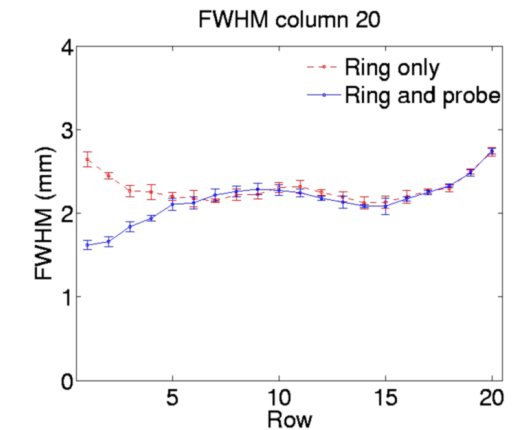
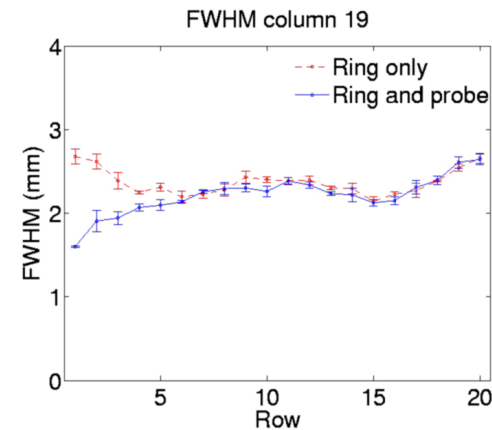
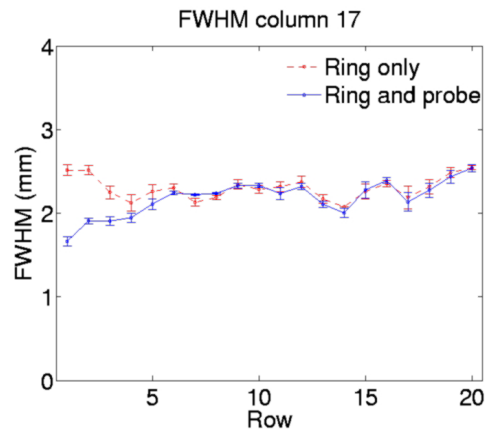
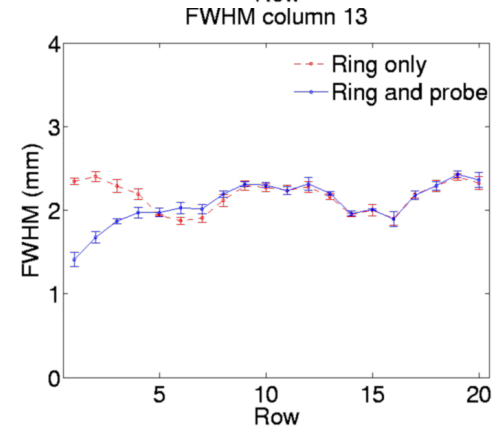
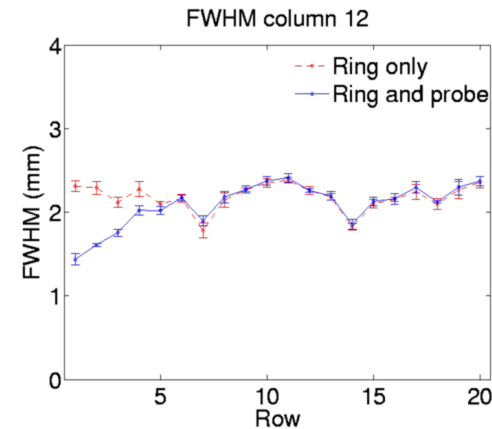
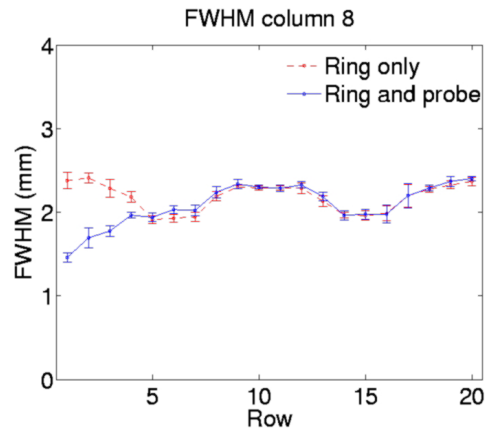
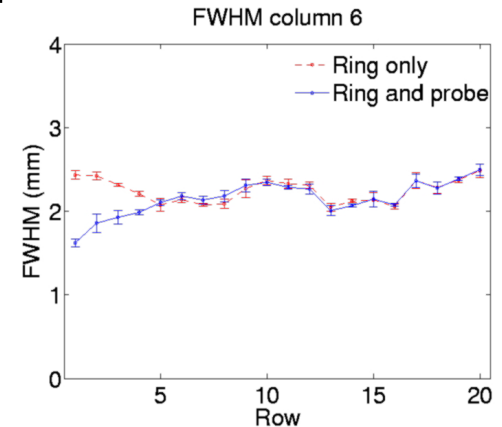
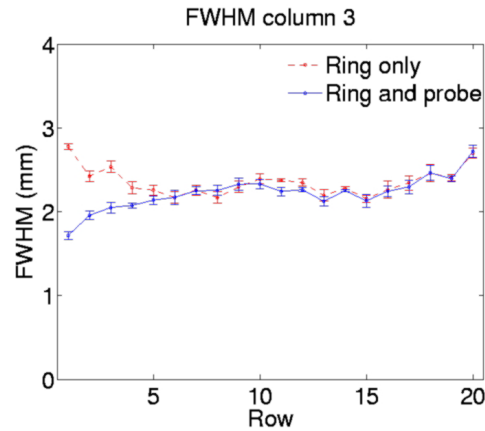
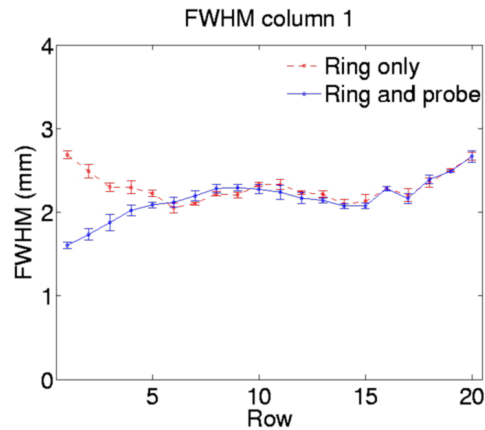
- SM elements weighted by Siddon length through probe
- Applied in only in Sensitivity correction, cancels elsewhere
- Successful in ring-ring and probe-ring images, fails in combined image

# Spatial resolution

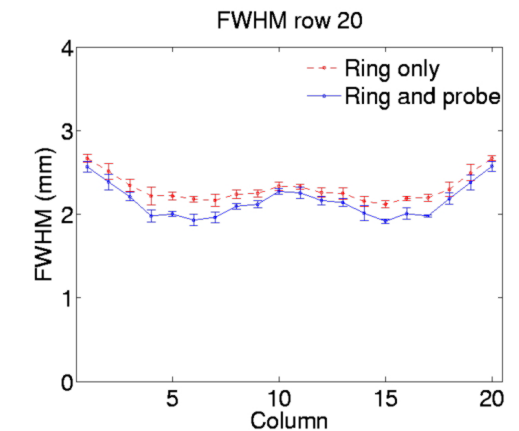
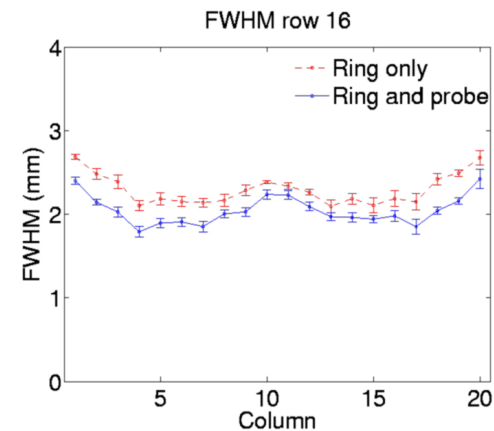
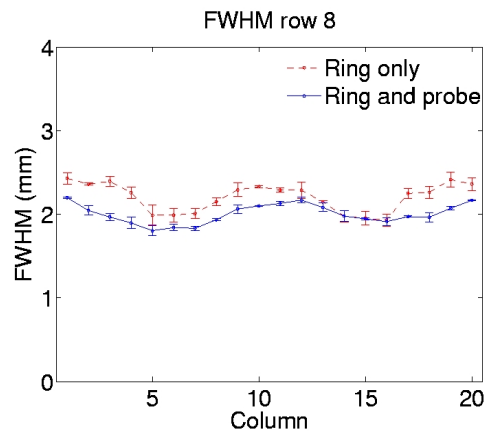
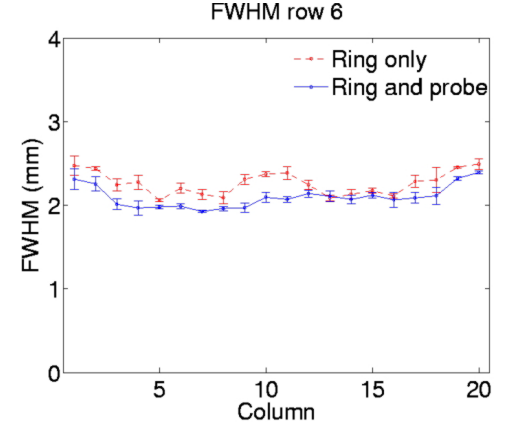
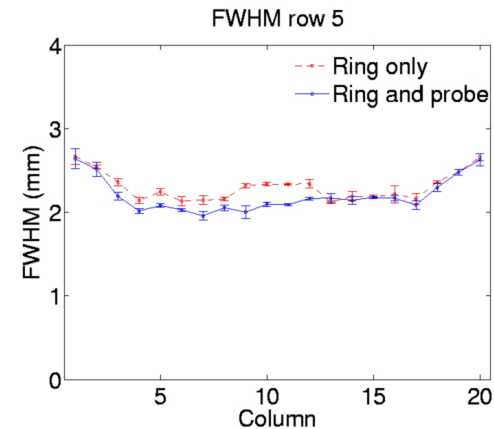
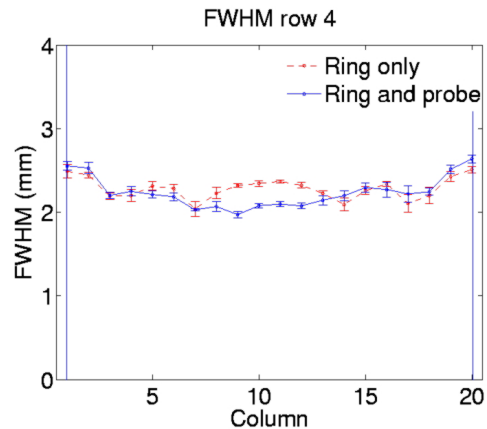
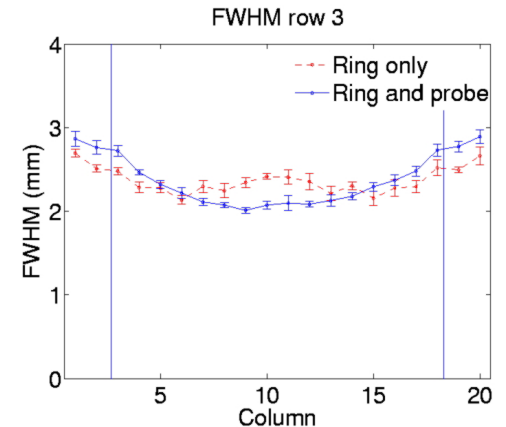
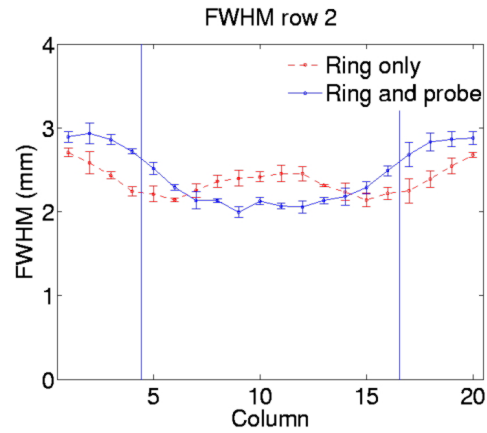
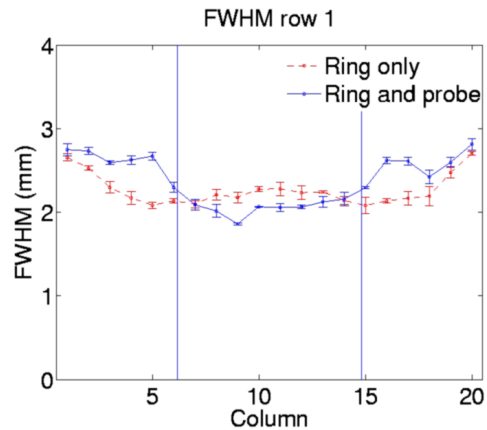
- System IRF non-isotropic, shift variant
  - Probe-ring LORs are fan-shaped
- Grid of points simulated
  - ...on low background (non-negativity, cold spot bias)



# Resolution perpendicular to the probe surface

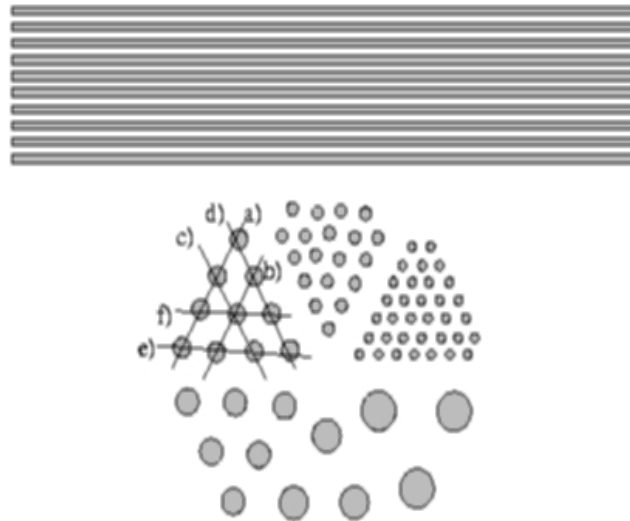


# Resolution parallel to the probe surface



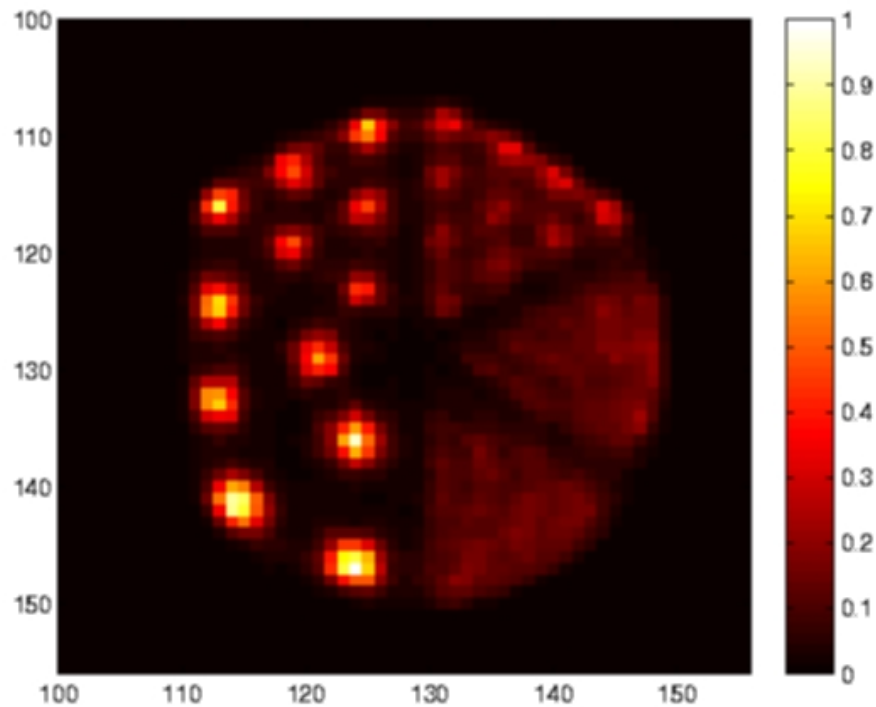
# Image studies

- Resolution phantom
  - Small derenzo inserts measuring 4.8, 4.0, 3.2, 2.4, 1.6 and 1.2 mm in diameter

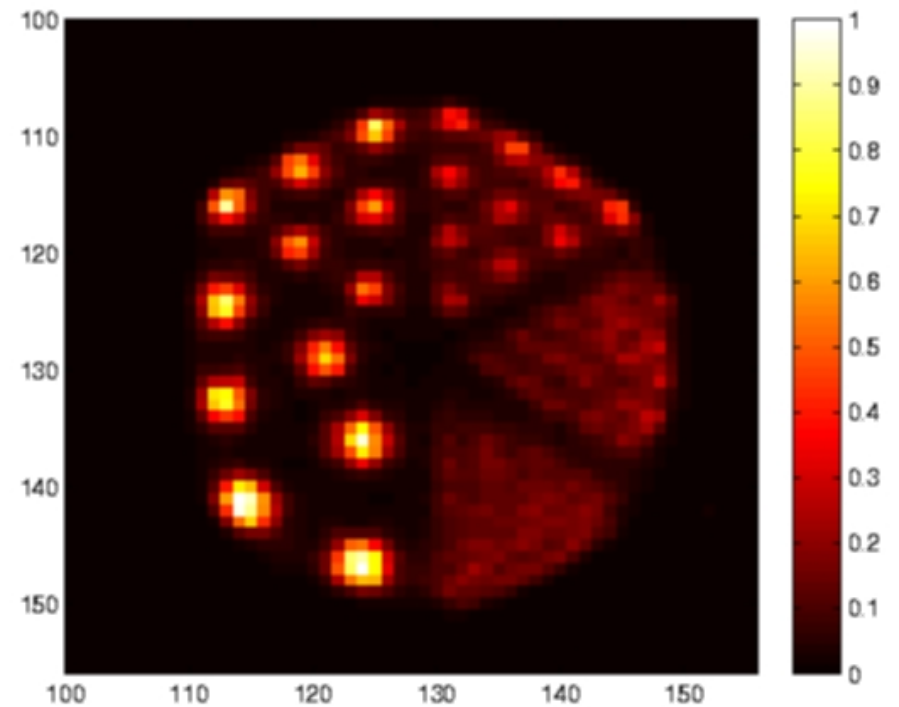


# Image studies

- Resolution phantom



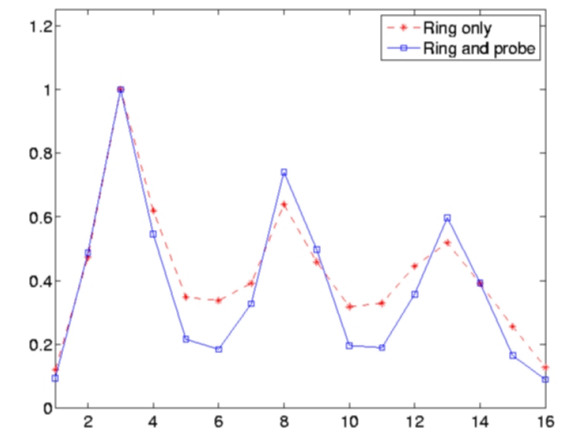
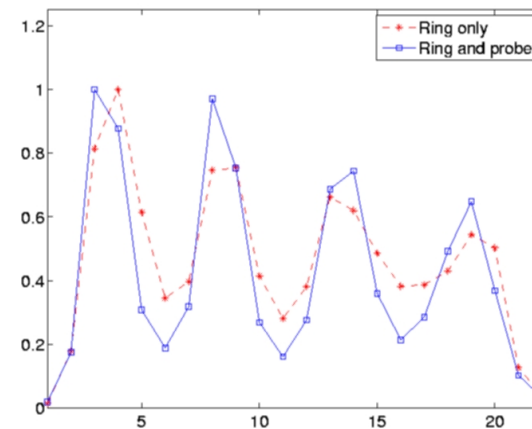
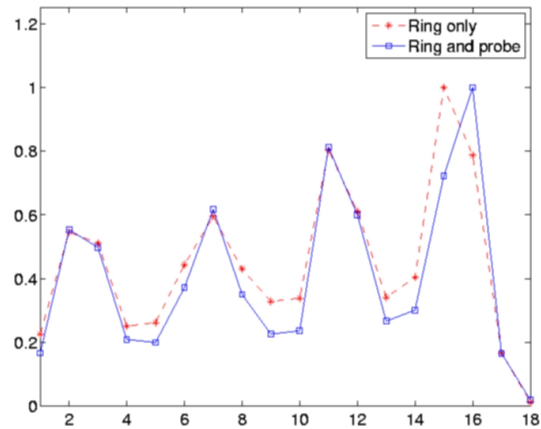
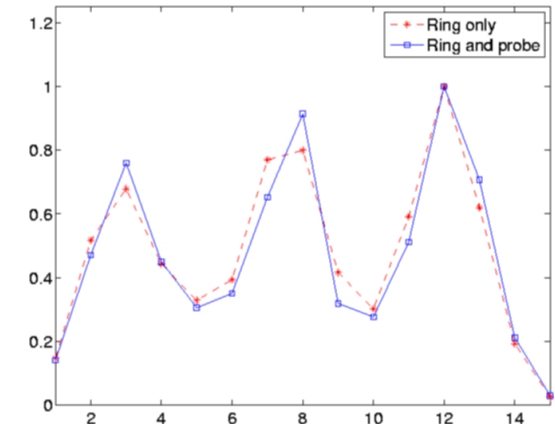
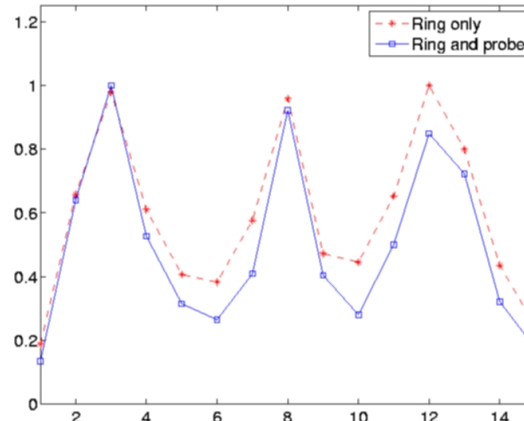
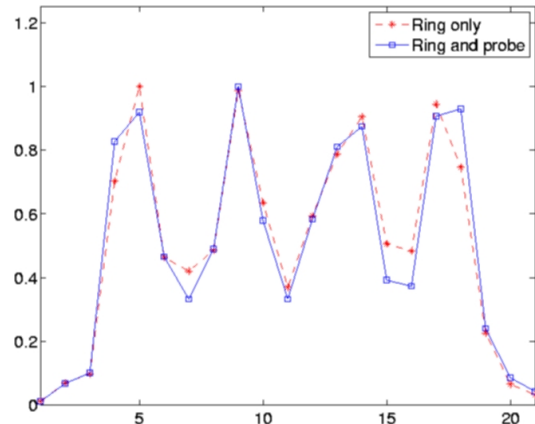
Ring only



Ring and probe

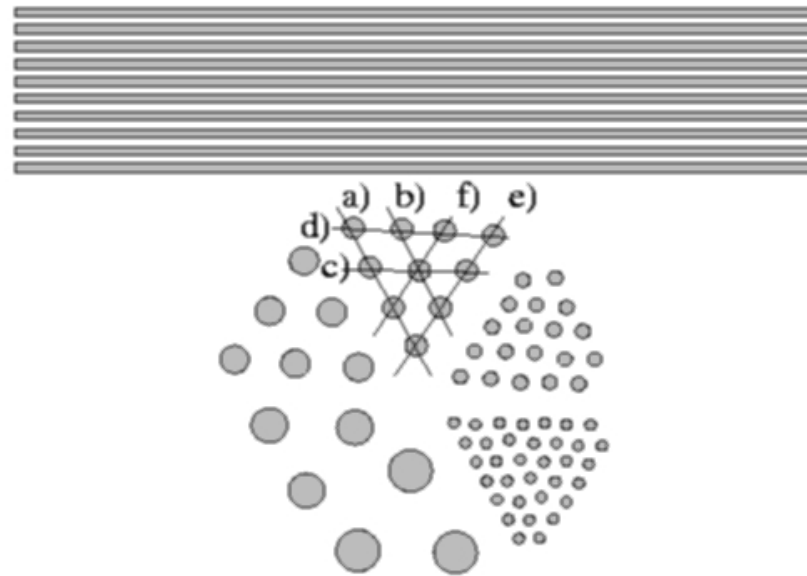
# Image studies

- Resolution phantom



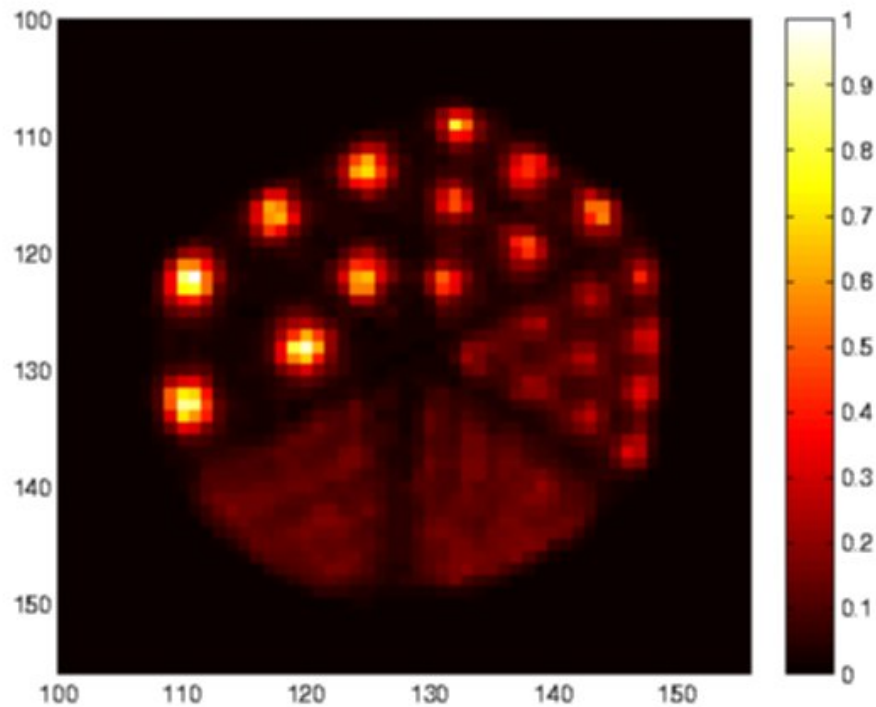
# Image studies

- Resolution phantom
  - Now the probe closer to the ROI

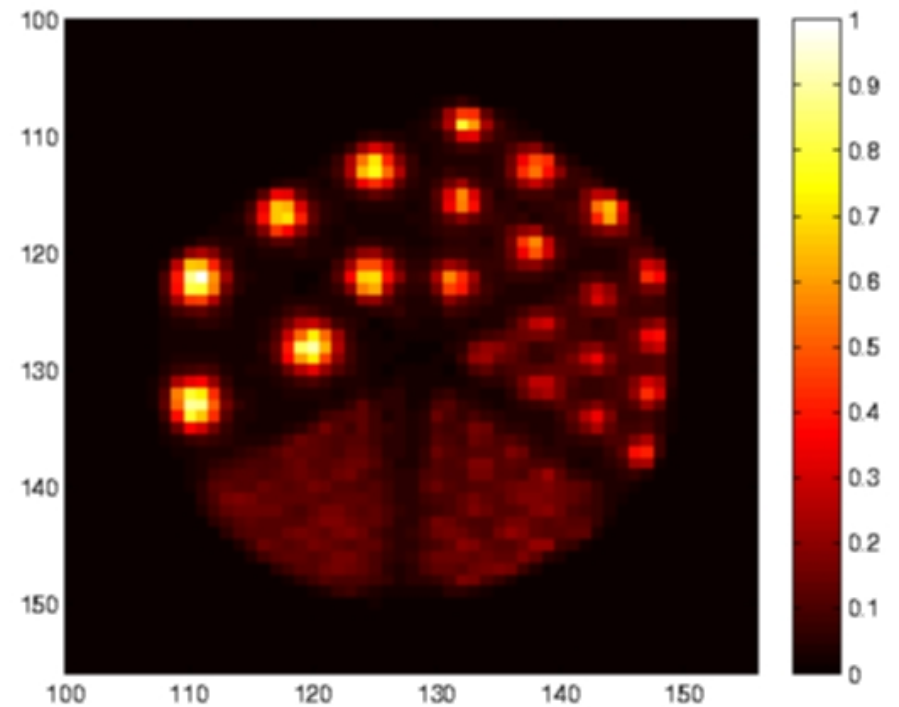


# Image studies

- Resolution phantom



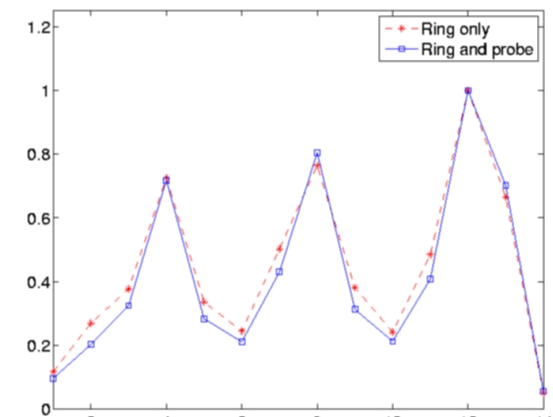
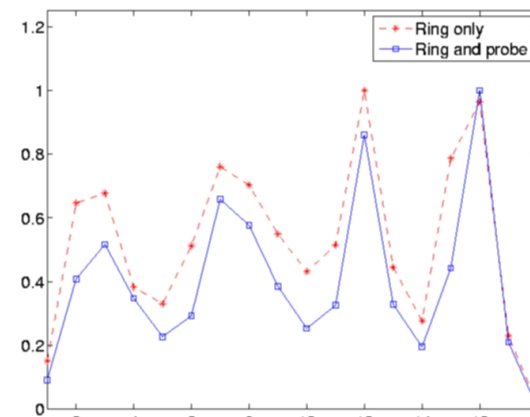
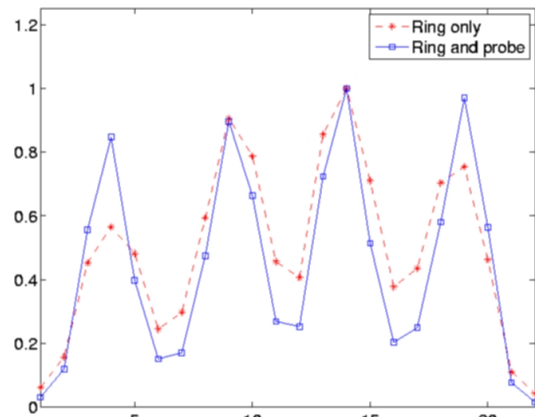
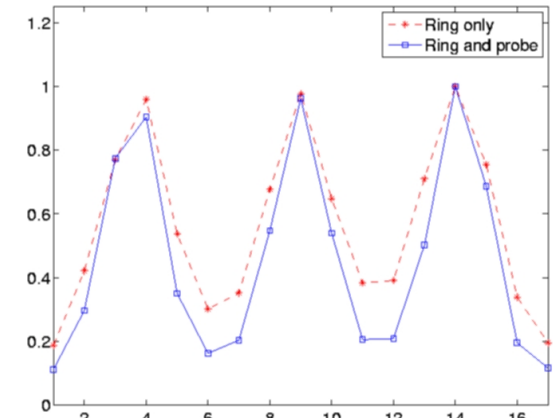
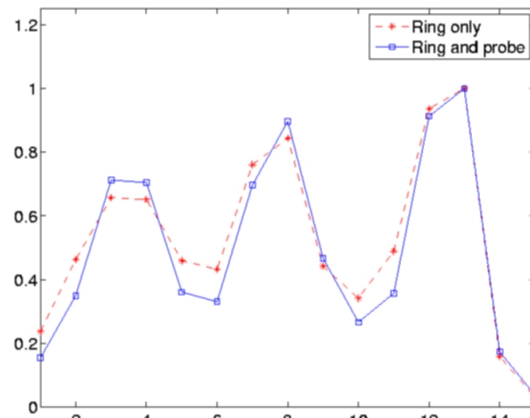
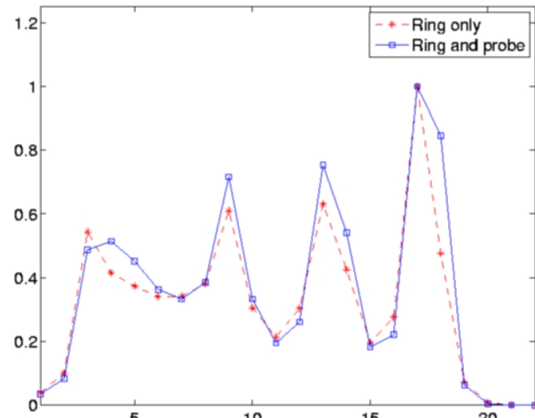
Ring only



Ring and probe

# Image studies

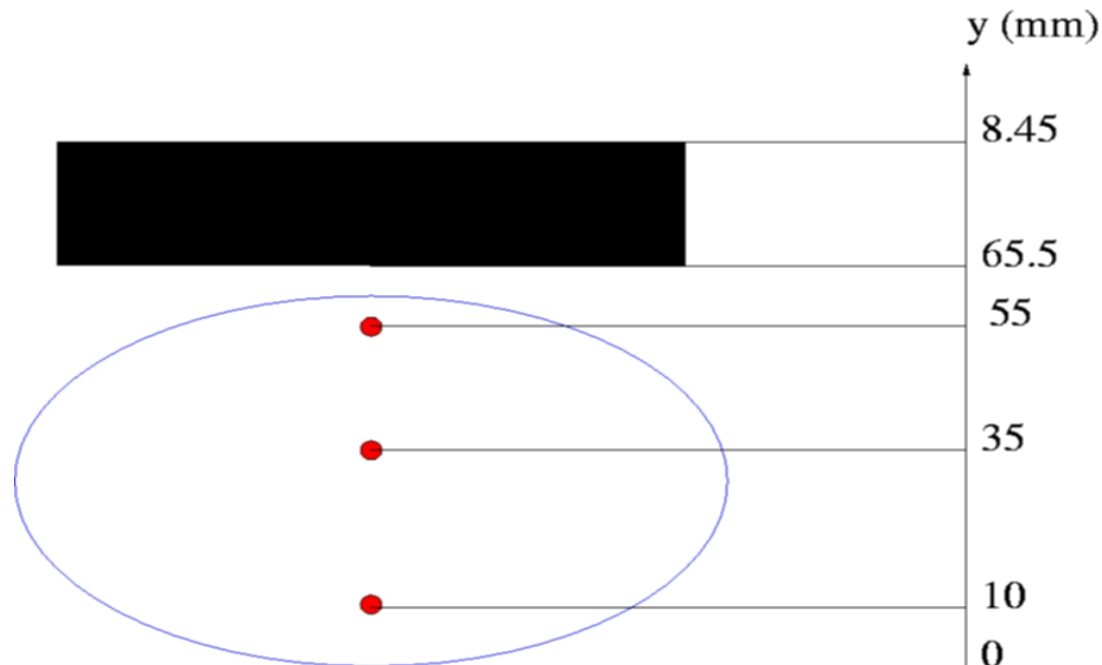
- Resolution phantom



# Image studies

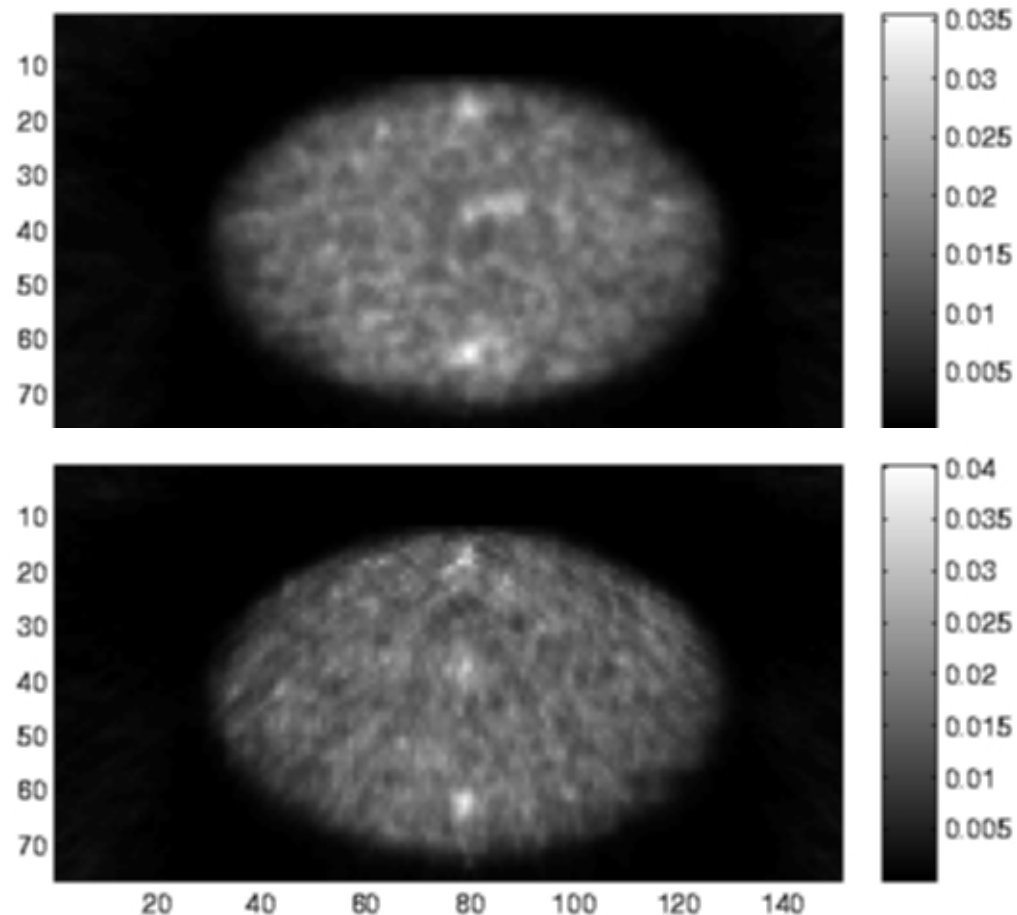
- Mammography application

- Breast phantom
- Three hot lesions (3 mm diameter) on a uniform background, varying distances from probe
- 8:1 uptake ration



# Image studies

- Mammography application
  - Post reconstruction filtering (gaussian, FWHM = 1 mm)

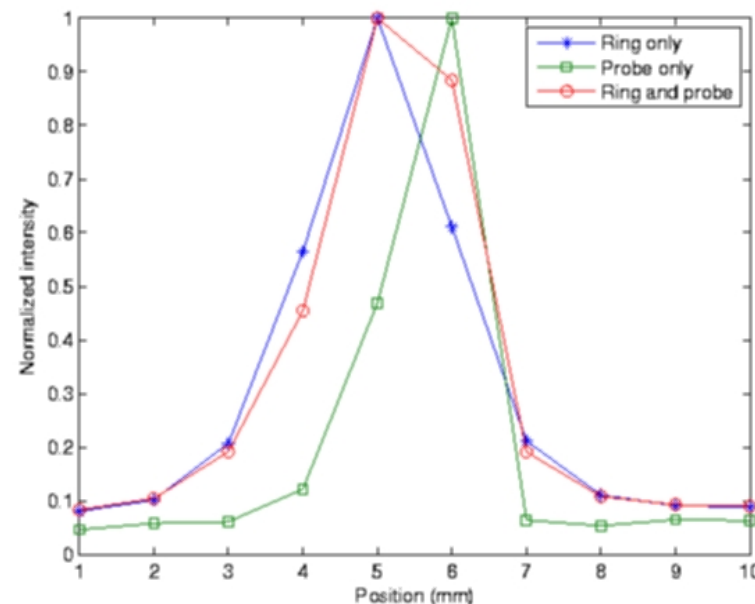


# Conclusions

- High-resolution PET-probe system presented
- IRF comparison show resolution improvement in ROI close to the probe
- Imaging studies using resolution phantom show improvement
- Application to mammography motivated by breast phantom imaging study

**Thank you for your attention!**

- FWHM not realistic, only for comparison
  - Scattering will affect results
  - Probe can be used to remove scattering events
- Loss of resolution at top corners of FOV -> DOI



# Discussion

- FWHM not realistic, only for comparison
  - Scattering will affect results
  - Probe can be used to remove scattering events
- Loss of resolution at top corners of FOV -> DOI
- Room for improvement
  - Better model -DOI, sampling for finer grid
  - Sensitivity correction
  - Compton camera -increase sensitivity